

## Atlas-Free Functional Brain Connectome Analysis via **Task-Driven Parcellation**

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## **SUMMARY**

Selecting a suitable brain atlas for node definition is a critical yet challenging step in functional connectome analysis. A mismatched atlas can obscure subtle topographies and undermine the subsequent analysis. In this work, we propose an Atlas-Free functional brain CONnectome analysis (AFCON) that bypasses atlas selection by jointly optimizing an adaptive parcellation module and a graph-based connectome analysis module. Unlike classical methods reliant on fixed, predefined atlases, AFCON adaptively generates task-specific, individualized parcellations from fMRI data, which better align with the prediction task and offer enhanced interpretability. In addition, we introduce two neurobiologically-informed regularizers to ensure plausible parcellations: a balanced distribution regularizer to mitigate extreme parcel size imbalances and a spatial compactness regularizer to promote anatomical coherence. Experiments on ADHD and ADNI datasets demonstrate that AFCON consistently matches or outperforms atlas-based baselines in terms of predictive accuracy while identifying disease-relevant brain regions, enhancing both interpretability and clinical relevance. Notably, this work focuses on the cerebral cortex, serving as an initial step towards potential whole-brain connectivity analysis in the future for more robust clinical utility.

## Framework

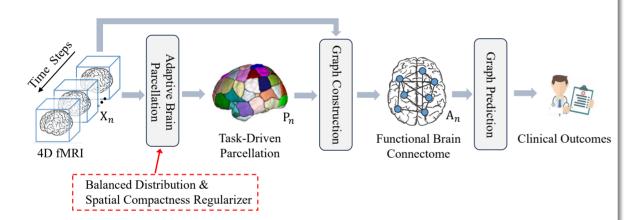


Figure: The Overall Framework of AFCON.

**Adaptive Brain Parcellation.** We apply a 3D U-Net to generate voxel-wise soft assignments of cortical voxels into K ROIs. During training, Gumbel-Softmax enables differentiable one-hot assignments; during inference, Argmax is used for deterministic parcellation.

To enhance biological plausibility, we introduce two regularizers:

Balanced Distribution Regularizer: Prevents extreme imbalances of ROI sizes by penalizing deviations from a uniform volume distribution:

$$\mathcal{L}_{\text{balance}} = \sum_{n} \text{KL}(\mathbf{p}_n \parallel \mathbf{u}), \quad \mathbf{u} = \begin{bmatrix} \frac{1}{K}, \dots, \frac{1}{K} \end{bmatrix}$$

where  $p_{n,k}$  is the proportion of cortical voxels assigned to ROI k for subject n.

Spatial Compactness Regularizer: Promotes geometric coherence of voxels within each ROI by minimizing spatial variance around soft centroids:

$$\mathbf{c}_{n,k} = \frac{\sum_{v} \mathbf{coord}_{v} \cdot s_{n,k}(v)}{\sum_{v} s_{n,k}(v)}, \quad \mathcal{L}_{\text{compact}} = \sum_{n,k} \frac{\sum_{v} s_{n,k}(v) \|\mathbf{coord}_{v} - \mathbf{c}_{n,k}\|^{2}}{\sum_{v} s_{n,k}(v)}$$

**Graph-based Connectome Analysis.** From the parcellation, ROI-wise time series are obtained by averaging voxel time courses. We compute functional connectivity matrices  $C_n$  using Pearson correlation and retain the top 10% positive connections to form sparse brain networks  $\mathbf{A}_n \in \mathbb{R}^{K \times K}$ . We adopt a Graph Convolutional Network (GCN) to predict target labels:

$$\hat{y}_n = GCN(\mathbf{A}_n, \mathbf{H}_n)$$

where  $\mathbf{H}_n$  is the connection profile node feature matrix (i.e., rows of  $\mathbf{C}_n$ ).

## EXPERIMENTS

**Datasets.** Two rs-fMRI datasets: ADHD-200 (569 subjects; 43.2% ADHD; 64 timepoints) and ADNI (200 subjects balanced between AD and HC; 197 timepoints), both preprocessed using fMRIPrep.

Table: Overall Prediction Performance (mean±std, %).

Model	ADHD			ADNI		
	ACC↑	AUC↑	<b>F1</b> ↑	ACC↑	AUC↑	<b>F1</b> ↑
GCN	$59.7_{\pm 6.2}$	$63.2_{\pm 6.9}$	$48.3_{\pm 12.7}$	$60.5_{\pm 9.1}$	$65.7_{\pm 9.2}$	$63.4_{\pm 8.3}$
GAT	$57.7_{\pm 2.9}$	$60.3_{\pm 3.7}$	$53.6_{\pm 10.0}$	$56.0_{\pm 2.5}$	$59.4_{\pm 9.1}$	$55.4_{\pm 5.7}$
BrainGNN	$53.2_{\pm 3.8}$	$55.2_{\pm 3.7}$	$50.3_{\pm 7.0}$	$51.0_{\pm 5.4}$	$52.3_{\pm 6.3}$	$53.2_{\pm 5.5}$
BrainNetCNN	$56.0_{\pm 3.3}$	$58.7_{\pm 6.4}$	$52.1_{\pm 6.7}$	$58.5_{\pm 4.6}$	$65.9_{\pm 7.8}$	$53.6_{\pm 19.1}$
BrainGB	$56.7_{\pm 2.7}$	$58.3_{\pm 4.4}$	$46.0_{\pm6.1}$	$56.5_{\pm 5.8}$	$59.7_{\pm 4.9}$	$58.2_{\pm 7.2}$
BrainNetTF	$59.8_{\pm 5.4}$	$63.8_{\pm 7.7}$	$45.0_{\pm 22.8}$	$59.5_{\pm 5.3}$	$62.3_{\pm3.8}$	$59.7_{\pm 8.6}$
NeuroGraph	$56.5_{\pm 5.4}$	$59.4_{\pm 4.3}$	$57.6_{\pm 4.7}$	$56.5_{\pm 8.5}$	$57.6_{\pm 8.2}$	$58.9_{\pm 11.1}$
AFCON (K=48)	$63.2_{\pm 2.7}$	$65.6_{\pm 2.1}$	$56.8_{\pm 3.5}$	$62.5_{\pm 6.5}$	$66.1_{\pm 7.3}$	$62.6_{\pm 5.7}$
AFCON ( <i>K</i> =90)	$60.0_{\pm 4.9}$	$63.5_{\pm3.1}$	$50.7_{\pm 12.0}$	$61.5_{\pm 4.1}$	$65.6_{\pm 5.6}$	$61.5_{\pm 5.9}$
AFCON ( <i>K</i> =200)	$61.8_{\pm 0.9}$	$62.9_{\pm2.0}$	$47.9_{\pm 6.8}$	$62.0_{\pm 5.1}$	$66.7_{\pm 4.2}$	$59.8_{\pm 7.5}$
AFCON ( <i>K</i> =360)	$61.1_{\pm 3.9}$	$63.4_{\pm 5.7}$	$49.8_{\pm 11.6}$	$59.5_{\pm 3.3}$	$65.1_{\pm 2.7}$	$55.1_{\pm 6.8}$

- AFCON consistently matches or outperforms baselines with lower variances, indicating improved accuracy and robustness.
- Parcellation resolution (i.e., ROI count) affects performance; careful selection is essential based on disease characteristics and research goals.

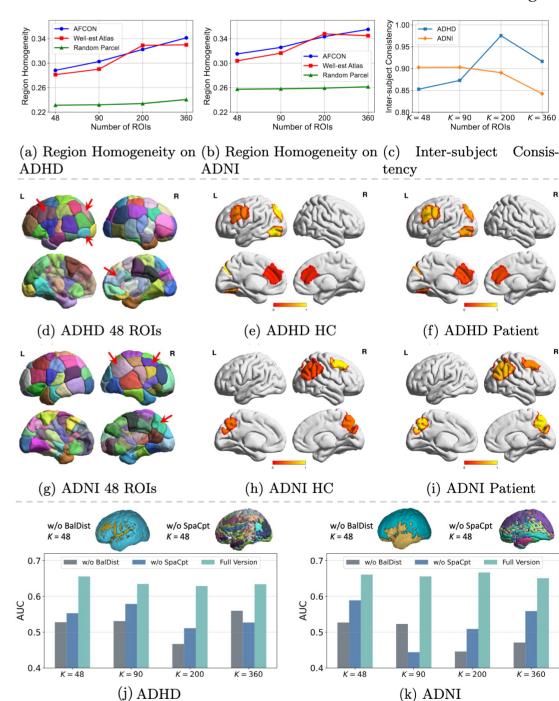


Figure: (a)-(c) Quantitative analysis of the learned parcellation. (d)-(i) highlight salient ROIs for ADHD and AD. (j)-(k) Ablation Study of the proposed regularizers.

- Fig (a)-(c) show that AFCON produces functionally coherent and consistent parcellations, and identifies clinically relevant regions aligned with known ADHD and AD pathology.
- Regularizers improve performance across cohorts. Balanced-Distribution contributes more to prediction gains in ADHD, while Spatial-Compactness has a notable impact in ADNI, suggesting that balanced ROI sizes help capture ADHD's diffuse dysconnectivity, whereas compact parcels better reflect the focal atrophy patterns in AD.